DEVELOPMENT AND VALIDATION OF A HEART ATLAS TO STUDY CARDIAC EXPOSURE TO RADIATION FOLLOWING TREATMENT FOR BREAST CANCER

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Purpose: Cardiac toxicity is an important sequela of breast radiotherapy. However, the relationship between dose to cardiac structures and subsequent toxicity has not been well defined, partially due to variations in substructure delineation, which can lead to inconsistent dose reporting and the failure to detect potential correlations. Here we have developed a heart atlas and evaluated its effect on contour accuracy and concordance.

Methods and Materials: A detailed cardiac computed tomography scan atlas was developed jointly by cardiology, cardiac radiology, and radiation oncology. Seven radiation oncologists were recruited to delineate the whole heart, left main and left anterior descending interventricular branches, and right coronary arteries on four cases before and after studying the atlas. Contour accuracy was assessed by percent overlap with gold standard atlas volumes. The concordance index was also calculated. Standard radiation fields were applied. Doses to observer-contoured cardiac structures were calculated and compared with gold standard contour doses. Pre- and post-atlas values were analyzed using a paired t-test.

Results: The cardiac atlas significantly improved contour accuracy and concordance. Percent overlap and concordance index of observer-contoured cardiac and gold standard volumes were 2.3-fold improved for all structures (p < 0.002). After application of the atlas, reported mean doses to the whole heart, left main artery, left anterior descending interventricular branch, and right coronary artery were within 0.1, 0.9, 2.6, and 0.6 Gy, respectively, of gold standard doses.

Conclusions: This validated University of Michigan cardiac atlas may serve as a useful tool in future studies assessing cardiac toxicity and in clinical trials which include dose volume constraints to the heart. © 2011 Elsevier Inc.

INTRODUCTION

Adjuvant radiotherapy is a standard component of breast cancer treatment, both in women undergoing breast conservation therapy and in patients at high risk for local-regional recurrence following mastectomy. With improved therapies, patients are often cured and survive long enough for long-term effects to become apparent. In the past several years, cardiac toxicity has been recognized as an important sequela of breast radiotherapy, particularly among patients treated for left-sided disease (1–3). Although investigators have found statistical correlations between patients who received breast radiotherapy and later developed cardiac disease, the specific relationships between doses to cardiac structures and subsequent toxicity have not been well defined, likely due in large part to variation in structure delineation. This can lead to inconsistent reporting of doses and failure to detect potential dose-volume correlations. In the era of systemic therapies, including anthracyclines and trastuzumab, which carry an independent risk of cardiac toxicity, any additional potential risk due to radiotherapy must be identified and kept to a minimum.

As a first step, we have developed a heart atlas and evaluated its effect on contour accuracy and concordance. We have included substructures including vessels, chambers, valves and the conduction system to allow for substructure identification and dose estimation in future studies.

Cardiac dysfunction, Breast cancer, Thoracic radiotherapy, Cardiac atlas, Normal-tissue sparing.

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METHODS AND MATERIALS

Development of cardiac atlas

A detailed cardiac computed tomography (CT) atlas was developed jointly by a cardiologist (TK), a radiologist (AC), and a radiation oncologist (MF). Images were obtained with respiratory gating with and without intravenous (IV) contrast. The whole heart (WH) was delineated, along with substructures including the chambers, great vessels, cardiac valves, the conduction system, and major coronary vessels. The contours were agreed upon by all three investigators and were considered to be the gold standard (GS) volumes for future reference. Written guidelines for consistent delineation, as noted below, were also jointly developed.

Validation of cardiac atlas

Seven radiation oncologists from the University of Michigan Health System who routinely treat breast cancer were recruited for this study. Two oncologists specialize in breast cancer treatment at the main hospital, and five oncologists treat multiple disease sites, including breast cancer, at affiliate clinics. A pre- and post-test study was designed using breath-hold CT scans obtained from 4 patients with left-sided breast cancer, using active breathing control, as part of an institutional review board-approved study. Patients were placed in a supine position on a breast board, with both arms raised above their heads. Radiopaque catheters were placed at the inferior portion of the clavicular head and midline. For breast conservation cases, catheters were also placed 1.5 cm inferior and lateral to breast tissue, but no further posterior than the mid-axillary line. For post-mastectomy cases, catheters were placed in similar positions based on the position of the contralateral breast. Breathing was suspended at 80% of deep inhalation, and CT images with and without IV contrast were obtained. Four sets of images, two with IV contrast and two without, were selected to represent the range of heart positions relative to the chest wall. Images were imported into our in-house treatment planning system (University of Michigan Planning [UM-PLAN]). Using each of the 4 cases, observers contoured the WH, left main (LM) artery, left anterior descending (LAD) interventricular branch, and right coronary artery (RCA) before and after studying the atlas. On the scans with IV contrast, observers also contoured the left and right ventricles. All contours were stored separately, so no observers had access to their previous contours or those of their peers. As previously noted, GS contours were generated by the primary investigator upon consultation and review by physicians from the departments of cardiology and cardiac radiology.

Contour accuracy was assessed by percent overlap of observer volumes with the GS volumes and the concordance index (CI), which was defined as the intersection of observer and GS volumes divided by the union of these volumes. A value of 1 indicates perfect concordance. To evaluate the dosimetric impact of potential changes in structure delineation, standard fields were applied to the CT scans to cover the breast tissue and regional nodes, including the supraclavicular, infraclavicular, and internal mammary nodes in interspaces one through three. The preplaced radiopaque catheters were used as guides with which to design beams for three-dimensional (3D) dosimetric plans. The intact-breast cases were planned with 6-MeV partially wide tangential fields and a supraclavicular field to a dose of 50 Gy. In addition to tangential and supraclavicular fields, the chest wall cases required a 9-MeV mediolateral electron field to encompass internal mammary nodes in interspaces 1 through 3. The medial electron field is routinely used in our clinics if the heart is deemed too anterior to allow for partial wide tangential fields. All fields delivered 50 Gy to the plan normalization point. Dose-volume histograms were generated for all contoured structures. Doses to observer-contoured cardiac structures were calculated and compared with GS contour doses by using the following formula: (dose to observer contour minus dose to gold standard contour) divided by dose to gold standard contour. All comparisons were evaluated using a two-sided paired t test with a p value of < 0.05 indicating a significant difference.

RESULTS

Cardiac atlas

A detailed cardiac atlas consisting of images with and without IV contrast and written instructions describing the anatomy were provided (Figs. 1 and 2). For optimal visualization of most structures on CT images, a level of 50 and a window of 500 Hounsfield units were recommended. For viewing cardiac vessels, a level of 50 and a window of 150 were suggested.

**Whole Heart and pericardium.** Superiorly, the WH starts just inferior to the left pulmonary artery. For simplification, a round structure to include the great vessels as well can be contoured. Inferiorly, the heart blends with the diaphragm. Since cardiac vessels run in the fatty tissue within the pericardium, they should be included in the contours, even if there is no heart muscle visible in that area. If contrast is administered, the superior vena cava (SVC) can generally be contoured separately from the WH. If this is not possible, or when working with a noncontrast scan, the superior vena cava can be included for simplification and consistency.

**Chambers.** (1) The left atrium is typically the most superior chamber on axial CT. It is located to the left and posterior to the pulmonary trunk and begins just inferior to the left pulmonary artery. (2) The left ventricle is typically anterior to and to the left of the left atrium. (3) The right atrium starts to the right of the aortic root superiorly. It moves significantly, so the size of the chamber often appears to change size from slice to slice on a non-cardiac-gated CT. (4) The right ventricle lies directly beneath the sternum and connects to the pulmonary trunk.

**Vessels.** (1) The LM coronary artery originates from the left side of the ascending aorta, inferior to the right pulmonary artery. (2) The LAD artery, interventricular branch, originates from the left coronary artery and runs in the interventricular groove between the right and left ventricles. If it is difficult to see, raising the level and lowering the window may help (e.g., level 50, window 150). (3) The left circumflex artery originates from the left coronary artery and runs between the left atrium and ventricle. This structure moves significantly with cardiac motion, so often the location can seem noncontiguous from axial CT slice to slice, as the position of the atroventricular (AV) groove changes. (4) The RCA originates from the right side of the ascending aorta. Due to the native heart position in the chest, on axial CT, it appears to start inferior to the left coronary artery. It moves significantly with cardiac motion, so often the location can seem noncontiguous from axial CT slice to slice, as the position of the AV groove changes.

**Valves.** (1) The aortic valve is found within the ascending aorta and seen in cross-section on axial CT. In a contrast scan,
Fig. 1. Cardiac atlas showing scans without IV contrast. Contours are illustrated in the right column, with unmarked images provided in the left column for reference. Colored outlines are explained in the key to Fig. 2.
Fig. 2. Cardiac atlas showing scans with IV contrast. Contours are illustrated in the right column, with unmarked images provided in the left column for reference.
the leaflets typically create a Y shape within the lumen of the vessel. (2) The pulmonic valve is found within the pulmonary trunk and is seen in cross-section on axial CT. In a contrast scan, the leaflets typically create an X shape within the lumen of the vessel. (3) The tricuspid valve is located between the right atrium and ventricle. It is difficult to see, but it is defined as the area where the blood pool is shared between the atrium and ventricle. Due to cardiac motion, this structure can appear to be noncontiguous from axial CT slice to slice. (4) The mitral valve is located between the left atrium and ventricle. It is difficult to see, but it is defined as the area where the blood pool is shared between the atrium and ventricle.

**Conduction system.** The AV node cannot be seen on CT, since it has the same signal intensity as the surrounding myocardium. It is located on the basal portion of interventricular septum and extends between the right atrium and ventricle.

**Validation study**

Utilization of the cardiac atlas improved contour accuracy for all structures by using both the percent overlap and the CI (Fig. 3). After application of the atlas, the heart and left ventricle achieved 91% and 92% overlap, respectively, with the GS (Table 1). For small structures not frequently contoured in clinical practice, such as the LM coronary artery and the RCA, the percent overlap doubled after application of the atlas, although the absolute percentage was still relatively low. The CI score also improved significantly for all structures (Table 2). The highest concordances were found for the WH and ventricles. For the WH, the CI increased from 0.76 ± 0.11 pre-atlas to 0.89 ± 0.03 post-atlas (p < 0.001).

Following the placement of radiation fields, dosimetric analysis indicated a significant improvement in the consistency of dose reporting for several structures, including the heart, the LM coronary and LAD arteries and the RCA and right ventricle (Table 3). The difference between the mean observer dose and the GS dose for the heart improved from 0.9 Gy pre-atlas to 0.1 Gy post-atlas (p < 0.001). Reported LM coronary artery and LAD dose improved from a difference of 1.7 Gy to 0.9 Gy (p = 0.005) and 3.9 Gy to 2.6 Gy (p < 0.001), respectively. Right ventricle dose also improved significantly from 1.1 Gy to 0.5 Gy (p = 0.008). There was no difference between the contrast and noncontrast scans in any metric we assessed.

**DISCUSSION**

In the past few years, cardiac toxicity following radiotherapy for breast cancer has been recognized as an important issue. In the meta-analysis performed by the Early Breast Cancer Trialists’ Collaborative Group that included 78 randomized trials, an excess risk of mortality from heart disease (rate ratio, 1.27) was found in patients who received adjuvant radiotherapy (4). Hooning et al. (1) studied the treatment-specific incidence of cardiovascular disease in 4,414 patients in the Dutch late-effects breast cancer cohort who had survived 10 years after treatment. Compared to the incidence in the total Dutch female population, the authors found that patients who received radiation to the internal mammary nodes as part of their treatment had an increased risk of myocardial infarction (hazard ratio [HR], 1.7), congestive heart failure (HR 2.7), and valvular dysfunction (HR 3.2).

Harris et al. (2) reported a retrospective review of 961 patients with stages I and II breast cancer who received radiotherapy between 1977 and 1994 at the University of Pennsylvania. With a median follow-up of 12 years, the authors found that 20 years after treatment, patients who received left-sided radiotherapy had higher rates of coronary artery disease (25% vs. 10%), myocardial infarction (15% vs. 5%), and cardiac deaths (6.4% vs. 3.6%) than patients who received right-sided radiotherapy.

Jagi et al. (3) examined the University of Michigan experience with over 800 stage I or II breast cancer patients treated with radiotherapy between 1984 and 2000 and compared rates of cardiac events between patients treated to the left and right side. On multivariate analysis, the side of the treated breast did significantly predict for cardiac events, as might be expected, as the dose to heart structures is usually higher for patients with left-sided than with right-sided breast cancer (3).

Most studies demonstrating an association between breast radiotherapy and cardiac morbidity are registry-based retrospective reviews, which depend on diagnosis codes and thus symptomatic cardiac toxicity. While these analyses provide some indication of radiation-associated morbidity and mortality, due to their retrospective nature, they may underestimate the true rates of cardiac damage. Prospective studies have been conducted to assess new cardiac perfusion defects in asymptomatic patients following radiation exposure. While new defects have not yet been clearly correlated with cardiac morbidity or mortality, they appear to be a consequence of cardiac exposure to radiation. In a study (5) of 294 patients who previously received at least 35 Gy of mediastinal radiation for Hodgkin’s disease and had no known cardiac disease, 21% had abnormal ventricular images at rest on stress echocardiography and radionuclide perfusion imaging, indicating prior myocardial injury. An additional 14% developed perfusion defects during stress testing (5). In another study (6) of 114 patients treated with radiotherapy for left-sided breast cancer, perfusion defects seen in rest-gated single-photon emission CT cardiac perfusion scans increased with time since the completion of radiotherapy, so that over 40% of patients developed a new defect by 2 years. Over 25% of these defects were associated with wall motion abnormalities. Importantly, there was a correlation between these abnormalities and the fraction of the left ventricle in the radiation fields (6). These two studies illustrate a potentially high rate of cardiac damage associated with radiotherapy.

After breast radiotherapy, the early focus has been on ischemic cardiac disease, and since the LAD artery is the closest major coronary vessel to tangential breast fields, it stands to reason that it may be most often affected. Correa et al. (16) retrospectively examined the results of cardiac stress tests and catheterizations for patients who were treated with breast radiotherapy at the University of Pennsylvania between 1977...
Fig. 3. Improvement in cardiac substructure delineation consistency with the use of the cardiac atlas. Panels 1 and 3 show pre-atlas contours of seven observers on two representative cardiac slices without IV contrast. The WH, RCA, and LAD coronary artery are displayed. Panels 2 and 4 show post-atlas contours on the same cardiac slices. Panels 5 to 8 show representative slices with IV contrast. The WH, RCA, LAD coronary artery, and right and left ventricles are displayed. Panels 5 and 7 are pre-atlas and 6 and 8 are post-atlas. Notice the improvement in consistency, especially in cardiac vessel delineation.
and 1994 and subsequently developed cardiac symptoms. The study found a higher percentage of stress test abnormalities in patients who received left- rather than right-sided radiotherapy (59% vs. 8%, respectively). Seventy percent of the abnormalities were in the LAD artery territory. Catheterization confirmed the majority of coronary stenoses to be in the LAD (7).

Although many studies of the cardiac toxicity of breast cancer have focused on ischemic disease, the detrimental effects of radiation on other cardiac structures such as the pericardium, myocardium, valves, conduction system, and autonomic system have also been described (Table 4) (8).

Table 1. Percent overlap of observer and GS contours

<table>
<thead>
<tr>
<th>Structure</th>
<th>Pre-atlas mean ± SD% (% range)</th>
<th>Post-atlas mean ± SD% (% range)</th>
<th>p value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Heart</td>
<td>79 ± 13 (50–99)</td>
<td>91 ± 4 (73–99)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Left main coronary artery</td>
<td>10 ± 22 (0–72)</td>
<td>22 ± 20 (0–67)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>LAD artery</td>
<td>35 ± 21 (0–77)</td>
<td>62 ± 16 (28–89)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Right coronary artery</td>
<td>11 ± 14 (0–49)</td>
<td>24 ± 18 (0.2–59)</td>
<td>0.002</td>
</tr>
<tr>
<td>Left ventricle</td>
<td>87 ± 11 (62–99)</td>
<td>92 ± 6 (79–99)</td>
<td>0.06</td>
</tr>
<tr>
<td>Right ventricle</td>
<td>65 ± 10 (55–80)</td>
<td>74 ± 8 (61–88)</td>
<td>0.003</td>
</tr>
</tbody>
</table>

Abbreviation: SD = standard deviation.

Autopsy studies have found significant fibrosis of the conduction systems, out of proportion to the amount of fibrosis that can be attributed to coronary artery disease alone (12).

Despite the known associations of radiation with long-term cardiac effects, no consistent dose-volume correlations have been found. This is likely due to the lack of detailed dosimetric studies with consistent cardiac substructure volume delineation. In this study, we created and validated an atlas which may be used in future efforts to determine such correlations and which can ultimately serve to set standard dosimetric limits to the heart. Initial data can be gathered not only from patients treated with radiotherapy for breast cancer but also for any thoracic malignancy including lung cancer and lymphoma.

Application of the atlas improved contour accuracy in all structures, as measured by percent overlap of observer and GS volumes and the CI. Post-atlas delineation of the WH and left ventricle volumes overlapped by more than 90%. However, despite a statistically significant improvement of greater than 2-fold, the absolute percent overlap and CI for the right and LM coronary artery volumes remained quite low, at 24%, 0.18, 22%, and 0.18, respectively. This is likely due to the small structure volumes (1–2 cc), which magnify the relative discrepancies in contours. In the recent Radiation Therapy Oncology Group (RTOG) breast cancer radiotherapy contouring study by Li et al. (15), the CI (referred to as percent overlap in that paper) reported was approximately 50% for the internal mammary nodes, which are also small structures (3.2 cc in the two cases in which these nodes were targeted).

Dosimetric analysis indicated that the observed improvement in contour accuracy resulted in improved dose-reporting accuracy for the WH, LM coronary artery, LAD, RCA, and right ventricle. The lack of improvement in dose reporting for the left ventricle likely is a result of excellent pre-atlas agreement within 0.25 Gy of the GS, so that a post-atlas improvement to within 0.15 of the GS was not statistically significant (p = 0.13). Despite the relatively low percent overlap and CI for the LM and right coronary arteries noted above, dose reporting was quite accurate, within 0.9 and

Table 2. Concordance index

<table>
<thead>
<tr>
<th>Structure</th>
<th>Pre-atlas mean ± SD index value (range)</th>
<th>Post-atlas mean ± SD index value (range)</th>
<th>p value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Heart</td>
<td>0.76 ± 0.11 (0.47–0.90)</td>
<td>0.89 ± 0.03 (0.72–0.94)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Left main coronary artery</td>
<td>0.05 ± 0.12 (0.0–0.50)</td>
<td>0.18 ± 0.16 (0.01–0.50)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>LAD artery</td>
<td>0.19 ± 0.11 (0.0–0.46)</td>
<td>0.34 ± 0.07 (0.30–0.47)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Right coronary artery</td>
<td>0.08 ± 0.10 (0.0–0.32)</td>
<td>0.18 ± 0.08 (0.03–0.39)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Left ventricle</td>
<td>0.75 ± 0.06 (0.62–0.84)</td>
<td>0.79 ± 0.05 (0.71–0.86)</td>
<td>0.04</td>
</tr>
<tr>
<td>Right ventricle</td>
<td>0.55 ± 0.08 (0.43–0.68)</td>
<td>0.65 ± 0.08 (0.55–0.78)</td>
<td>&lt;0.001</td>
</tr>
</tbody>
</table>

Abbreviation: SD = standard deviation.

Table 3. Mean absolute value

<table>
<thead>
<tr>
<th>Structure</th>
<th>Pre-atlas (mean ± SD) dose difference (Gy)</th>
<th>Post-atlas (mean ± SD) dose difference (Gy)</th>
<th>p value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Heart</td>
<td>0.88 ± 0.15 (0.14–1.14)</td>
<td>0.14 ± 0.14 (0.00–0.26)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Left main coronary artery</td>
<td>1.68 ± 1.53 (0.88–1.56)</td>
<td>0.88 ± 1.56 (0.88–1.56)</td>
<td>0.005</td>
</tr>
<tr>
<td>LAD artery</td>
<td>3.90 ± 2.80 (2.56–3.31)</td>
<td>2.56 ± 3.31 (2.56–3.31)</td>
<td>&lt;0.001</td>
</tr>
<tr>
<td>Right coronary artery</td>
<td>1.15 ± 1.07 (0.61–1.39)</td>
<td>0.61 ± 1.39 (0.61–1.39)</td>
<td>0.001</td>
</tr>
<tr>
<td>Left ventricle</td>
<td>0.25 ± 0.20 (0.15–0.14)</td>
<td>0.15 ± 0.14 (0.15–0.14)</td>
<td>0.13</td>
</tr>
<tr>
<td>Right ventricle</td>
<td>1.06 ± 0.73 (0.46–0.37)</td>
<td>0.46 ± 0.37 (0.46–0.37)</td>
<td>0.008</td>
</tr>
</tbody>
</table>

Abbreviation: SD = standard deviation.

* Table shows mean absolute value (i.e., observer contour dose – GS dose [Gy]).
### Table 4. Spectrum of radiation damage to the heart*

<table>
<thead>
<tr>
<th>Structure</th>
<th>Abnormality</th>
<th>Natural history</th>
<th>Pathology</th>
</tr>
</thead>
<tbody>
<tr>
<td>Pericardium</td>
<td>Pericarditis</td>
<td>Chronic asymptomatic effusion and/or pericarditis with symptoms: hemodynamic compromise with either constriction or tamponade</td>
<td>Fibrous thickening and fluid production</td>
</tr>
<tr>
<td>Myocardium</td>
<td>Myocarditis</td>
<td>Progressive diastolic dysfunction and restrictive hemodynamics with symptoms: CHF</td>
<td>Diffuse interstitial fibrosis/ microcirculatory damage leading to capillary obstruction/ extensive fibrosis</td>
</tr>
<tr>
<td>Endocardium</td>
<td>Valvular damage</td>
<td>Over time, progressive stenosis and regurgitation</td>
<td>Cusp and/or leaflet fibrosis</td>
</tr>
<tr>
<td>Vascular System</td>
<td>Arteritis</td>
<td>Premature CAD/accelerated atherosclerosis</td>
<td>Ostial and proximal stenosis; LAD, RCA, and left main more than left circumflex</td>
</tr>
<tr>
<td>Conduction System</td>
<td></td>
<td>Pulmonary hypertension</td>
<td>Pathology similar to atherosclerosis</td>
</tr>
<tr>
<td>Autonomic Dysfunction</td>
<td>All forms of heart block and conduction delay Supraventricular tachycardia; heart rate variability</td>
<td>Fibrosis of conduction system</td>
<td></td>
</tr>
</tbody>
</table>

* Abbreviations: CHF = congestive heart failure; CAD = coronary artery disease.


0.6 Gy of the GS, respectively. This is likely due to the relatively low doses and gradual dose gradients that are seen near these structures with 3D breast radiation fields. It is possible that if applied to treatment plans for intrathoracic malignancies or intensity-modulated radiotherapy plans, dose-reporting accuracy could improve for all or a different combination of structures, depending on the location of the targets and the steepness of dose fall-off. Use of IV contrast did not improve contour accuracy or dose reporting, which is reassuring, since many centers do not routinely administer this for simulation scans. However, caution must be used if extrapolating to images obtained using older CT scanners, since the image quality may not be ideal.

This study serves as the first step toward gaining a deeper understanding of radiation effects on the heart. Correa et al. (16) examined potential predictive factors for development of cardiac disease after left-sided radiotherapy. However, the dosimetric factors considered were rudimentary and consisted of central lung distance and maximum heart width and length in the tangential radiation beams. No dose-volume parameters were studied (16). In 1996, Gagliardi et al. (17) determined a dose-response curve for the heart and myocardium based mainly on 3D reconstruction of 2D treatment plans, so the resulting dose-volume histograms on which the model was based were likely not very accurate.

Formal normal tissue complication probability models have been constructed for many organs including lung and liver for use in thoracic and abdominal tumor treatment planning, and formal dose-volume relationships have recently also been derived for the parotid and submandibular glands and pharyngeal constrictors in head and neck radiotherapy (18–21). With such information, treatment can be planned to stay below dose-volume parameters which may be expected to cause toxicity. Using consistent structure delineation, and therefore consistent dose reporting, we should be able to determine similar relationships for cardiac substructures and start to incorporate them into treatment planning.

Atlases have been developed for several disease sites in order to standardize target delineation. Examples include head and neck, prostate, rectal, and gynecologic malignancies, all developed through the RTOG. Early in 2009, the RTOG also finalized a breast radiotherapy atlas. However, the organ-at-risk delineation is also important. The RTOG finalized a branchial plexus atlas in 2009. In the RTOG breast atlas, the WH is included, but it is likely that cardiac substructures are also important as we begin to understand the effects of radiotherapy on cardiac function. Thus, we have devised and validated a more detailed atlas, which can also be used to assess the toxicity of radiotherapy for any thoracic malignancy.

Although this study is a strong first step, there are limitations to the direct application of our atlas to clinical practice. Our CT images were not obtained using cardiac gating so structure contours were likely slightly blurred due to motion. The overall magnitude of this is small but relatively more pronounced for small structures such as the LM coronary artery. The atlas was developed using respiratory-gated CT images to eliminate the major motion component, but respiratory gating may not be routinely used in most centers for breast radiotherapy planning or treatment, although it is more often used for lung cancer. To most accurately assess dose to cardiac substructures, either treatment must be delivered in a single breath hold state or we must have complete temporal-spatial information on these substructures to account for various positions relative to isodose lines.

**CONCLUSIONS**

We have developed a cardiac atlas and validated its effectiveness in improving the accuracy and concordance of contours, which led to improved dose-reporting accuracy. This atlas can be applied not only to breast cancer treatment but also to any treatment which could potentially deliver
radiation to a portion of the heart. Using consistent guidelines for structure delineation, we can begin to understand any causative effects of radiotherapy on cardiac morbidity and mortality with the goal of minimizing these risks in the future with multiinstitutional clinical trials which include dose-volume constraints on the heart and its substructures.

REFERENCES